

# Implementation of hybrid filter technique for noise removal from medical images

Shruti Bhargava Choubey\*, S.P.V. Subba Rao

Sreenidhi Institute of Science & Technology, Hyderabad.

\*Corresponding author E-mail: [shrutibhargava@sreenidhi.edu.in](mailto:shrutibhargava@sreenidhi.edu.in)

## Abstract

Image denoising is used to eliminate the noise while retaining as much as possible the important signal features. The function of image denoising is to calculate approximately the original image form the noisy data. Image denoising still remains the challenge for researchers because noise removal introduces artifacts and causes blurring of the images. Image denoising has become an essential exercise in medical imaging especially the Magnetic Resonance Imaging (MRI). MR images are typically corrupted with noise, which hinder the medical diagnosis based on these images. The presence of noise not only causes as undesirable visual quality as well as lowers the visibility of low contrast objects. In this paper noise removal approach has proposed using hybridization of three filter with DWT method.

Results calculated in terms of PSNR, MSE & TIME.

**Keywords:** PSNR, MSE, DWT, BVS, MAPE, MD.

## 1. Introduction

In day-to-day life, digital images have a key role in the area of computer aided tomography, aerial communications, telecommunication images, synthetic aperture radar, geographical information systems, astronomy etc. In diverse fields, mentioned above, scientists are facing the problem of recovering original images from incomplete, indirect and noisy images. Images get corrupted during acquisition by camera sensors, receivers, environmental conditions, improper lightning, undesirable view angle etc., [2]. A noisy image appears as spotted, granular, hoary image. Therefore, the problem of recovering an original image from noisy image has received an ever increasing attention in recent years [3]. The recovery of image can be accomplished by image denoising, a process of estimating the desired image from a corrupted image [4,5]. Image denoising is a course of action in digital image processing aimed at the removal of noise. The most important reason to diminish noise is that extraneous features will otherwise cause successive errors in recognition. Another motivation is that noise reduction reduces the size of the image file, and this in contrast reduces the time required for successive processing and storage. The purpose in the design of a filter to diminish noise is that it remove as much of the noise as possible while maintaining all of the image qualities. Noise is inevitably introduced to medical images due to various factors in medical imaging which degrades the quality of images, not clearly visible boundaries and structural details are not clearly visible, thus causes difficulties to medical diagnosis. Also there is a tradeoff between time/spatial resolution and signal to noise ratio (SNR). Practically acquisition time in medical imaging is limited due to patient comfort and system requirement. Therefore, fast imaging is needed. But when the time resolution is improved, the noise may cause the quality of images to be degraded, blurring boundaries and suppressing structural details, thus bring

difficulties to medical diagnosis. Therefore, the important factor that medical image de-noising adhere is to remove the noise while preserving important features [8].

## 2. Literature survey

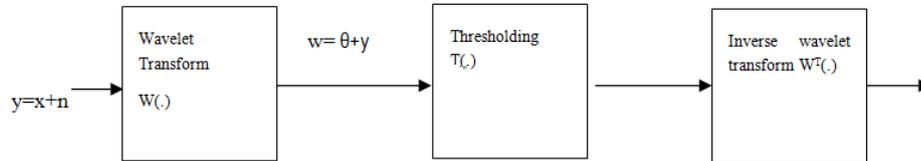
THE literature review summarizes, interprets and evaluates existing "literature" (published or available material) in order to establish current knowledge of a subject. The reason for doing literature survey is to relate to ongoing research to develop that knowledge. SOME paper investigates the suitability of different wavelet bases and the size of different neighbourhood on the performance of image de-noising algorithms in terms of PSNR and the image de-noising using discrete wavelet transform is analyzed. The experiments were conducted to study the suitability of different wavelet bases and also different window sizes. Among all discrete wavelet bases, *coif* let performs well in image de-noising [14].

**D.Giaouris, J.W.Finch** [15] showed that the denoising scheme based on the WT did not distort the signal and the noise component after the process was found to be small. But this process imposed a certain delay on the signal and was relatively complicated. In fixed frequency case, no improvement had been noted.

**Manish Goyal, Glenetan singh sekhon** [3] In this paper, a hybrid method is proposed for removing speckle noise from the image. Proposed method consist of two wavelet thresholding techniques: first technique by using statistical method and second technique based on bayes threshold. Result of both method is averaged and apply threshold for soft thresholding. For post processing wiener filter is used. It has been observed that combination of this method does perform better than the existing techniques. In wavelet based techniques edge preservation is also good and better speckle noise

suppression.

**Sudipta Roy, Nidul Sinha, Asoke K. Sen** [6] In this paper A new model based on the hybridization of wavelet and bilateral filters for denoising of variety of noisy images is presented . The model is experimented on standard images, like x-ray images, ultrasound and astronomical telescopic images and the performances are evaluated in terms of peak signal to noise ratio (PSNR) and image quality index (IQI). Results demonstrate that use of bilateral filters in combination with wavelet thresholding filters on subbands of a decomposed image deteriorates the performance.



**Fig. 1:** Block diagram for DWT based denoising framework

A similar approach can be applied to a speckle SAR image. The wavelet decomposition process is iterated with following approximations being decayed in turn, so that the image is broken down and represented by a small number coarser component in the lower spectral band (LL block) and a large number of detailed components in the higher spectral band (LH, HL and HH blocks). In broad-spectrum a signal has its energy concentrated in a small numeral of coefficients, while noise has its energy spread across over a large number of coefficients. Hence, through suitable thresholding or wavelet shrinkage of the higher spectral bands components (where the noise predominantly lies) we can greatly reduce or remove the noise speckle of the image in a wavelet domain. Since the noise characteristics can be different in each higher spectral block, each block will have to be thresholded separately according to its local noise variance. Finally, the thresholded coefficients are used in a wavelet reconstruction process to retrieve the speckle-reduced image with little loss of detail.

#### Algorithm for Denoising

I=Input Image

Taking I into the Denoising Block

Convert I from RGB to Gray Colour MAP say Igray

(Because the multidimensional matrix not supported by many digital filters & functions)

Let,  $dwt$ =Wavelet transform and  $THfilt$ =Wavelet filtering with respect to threshold

$(cA, cH, cV, cD) = dwt(Igray);$

Here, cA, cH, cV and cD are approximation, Horizontal, Vertical and Diagonal Coefficients respectively.

Update the approximation coefficients by filtering it.

$cA = THfilt(cA);$

$THfilt$  is the thresholding function that we considered, by taking following points as a filtering criteria

- Eliminate in the wavelet representation those elements with small coefficients, and
- Decrease the impact of elements with large coefficients.
- In mathematical terms, all we are doing is thresholding the absolute value of wavelet coefficients by an appropriate function.

Similar operation will be perform for multi-level decomposition

For second level

$(cA1, cH, cV, cD) = dwt(cA);$

$cA1 = THfilt(cA1);$

For third level  $(cA2, cH, cV, cD) = dwt(cA1);$

$cA2 = THfilt(cA2);$

After the transformation procedure, we have to apply inverse transform on the input medical image Let,  $idwt$ =Inverse Wavelet Transform of data

### 3. Proposed method

Given a noisy signal  $y = x + n$  where  $x$  is the desired signal and  $n$  is independent and identically distributed (*i.i.d*) Gaussian noise  $N(0, \sigma^2)$ ,  $y$  is first decomposed into a set of wavelet coefficients  $w = W[y]$  consisting of the required coefficient  $\theta$  and noise coefficient  $n$ . By applying a suitable threshold value  $T$  to the wavelet coefficients, the desired coefficient  $\theta = T[w]$  can be obtained; Lastly an inverse transform on the desired coefficient  $\theta$  will generate the denoise signal  $x = W^T[\theta]$ .

$Y2 = idwt(\text{with respect to } cA2 \text{ \& other parameters are kept same});$   
 $Y1 = idwt(\text{with respect to } cA1 \text{ \& other parameters are kept same});$   
 $Y = idwt(\text{with respect to } cA \text{ and } cDu \text{ \& other parameters are kept same});$

Here, Updated Diagonal coefficients are calculated as

$cDu = \text{mean of } cD \text{ \& } cH$

Let, median, average and diffusion are median, average and diffusion filters for data filtering.

$Ym = \text{Median}(Y);$

A median filter is more effective than convolution when the goal is to simultaneously reduce noise and preserve edges.

Create a filter structure for average filter, Say  $FSA$ , after that, we have to perform multidimensional filtering on median filtered data, according to the specified options for average filter.

$Ya = \text{Filter}(Ym, FSA);$

Numerical gradient calculations is perform from average filtered output, say by function *Gradient*

$fx, fy = \text{Gradient}(Ya)$

After that, we have to calculate discrete Laplacian of the average filtered image, in order to pass it through diffusion approximation with two dimensional gradient functions. Say, *Diffusion* is the function involving whole process of anisotropic diffusion which we have to apply on average filtered data, reducing image noise without removing significant parts of the image content, typically edges, lines or other details that are important for the interpretation of the image.

$Yd = \text{Diffusion}(Ya);$

Here,  $Yd$  is the final output that we are taking from denoising block which we use further in segmentation block As a consequence, the resulting medical images preserve linear structures while at the same time smoothing is made along these structures. Both these cases can be described by a generalization of the usual diffusion equation where the diffusion coefficient, instead of being a constant scalar, is a function of image position and assumes a matrix (or tensor).

### 4. Result & discussion

As a first we implemented basic discrete wavelet transform based denoising and calculated the efficiency in terms of MSE and PSNR. In order to overcome the ill influence of noise and shading, there is a need to take them into consideration when selecting the threshold being used. On the other hand, this is an impossible mission in a global context, since no one threshold can fit the entire image. This leads to the conclusion, that a more local threshold must be used. The locality property can allow a few cautious assumptions, and according to them produce a suitable threshold for the pixels in the environment.

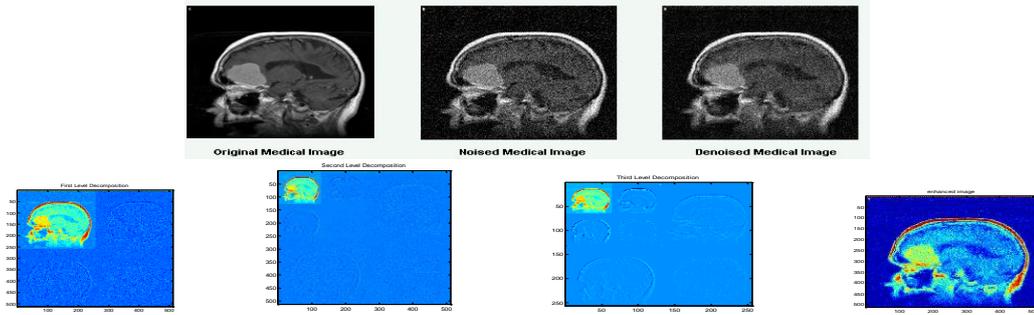


Fig. 2: (a) (b) (c) Different level of wavelet decomposition. (d) enhanced image

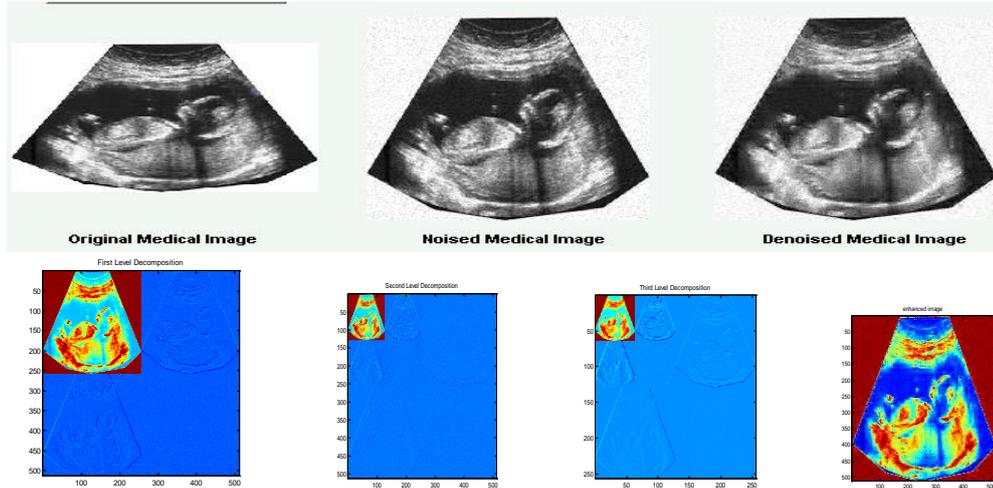


Fig. 3: (a) (b) (c) Different level of wavelet decomposition (d) Enhanced image

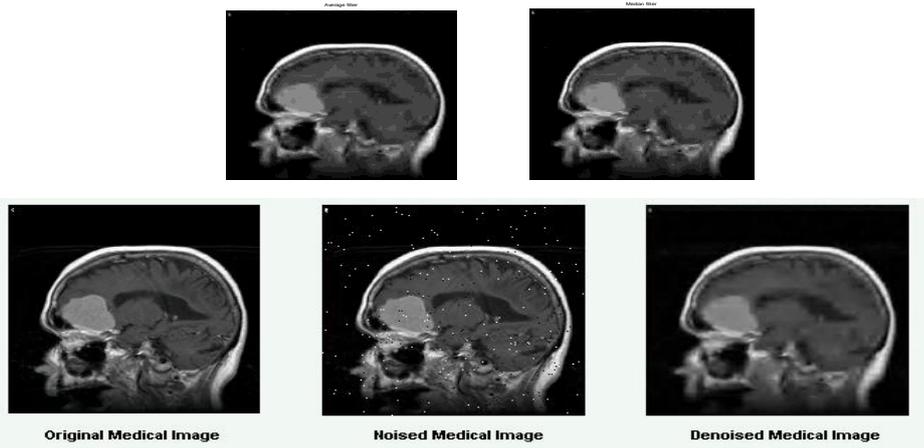


Fig. 4: Resultant image after a (Median filter), b (Average filter), c (Diffusion filter) final denoised image)

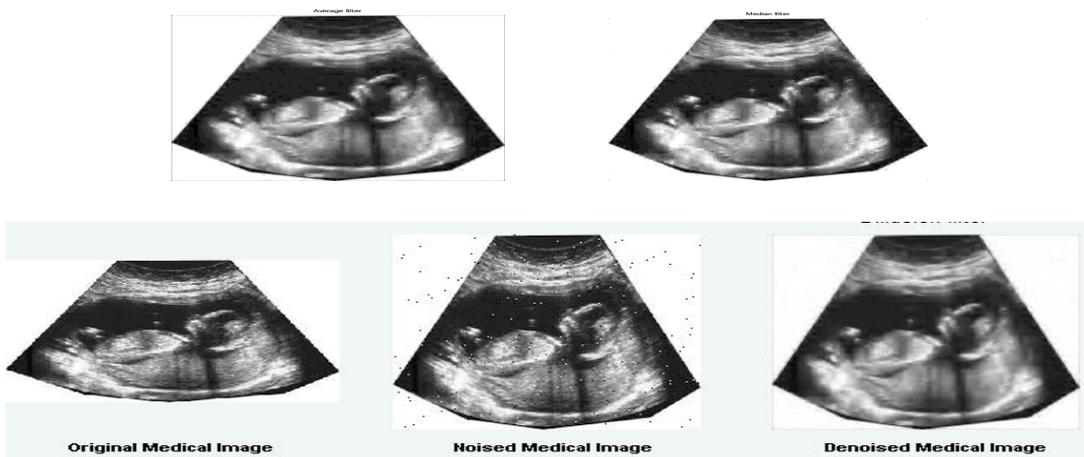


Fig. 5: Resultant image after a (Median filter), b (Average filter), c (Diffusion filter final denoised image)

Table 1: Table Showing Different PSNR, MSE, WPSNR, SSIM and Run Time for Image 1

Salt & Pepper	PSNR	MSE	WPSNR	SSIM	TIME
DWT	33.98	25.96	34.93	0.6171	9.33
Filters	34.25	24.41	32.85	0.779	4.15
Gaussian	PSNR	MSE	WPSNR	SSIM	TIME
DWT	31.57	45.29	32.65	0.5038	0.577
Filters	34.26	24.36	32.9	0.5684	1.147
Speckle	PSNR	MSE	WPSNR	SSIM	TIME
DWT	33.44	29.43	34.83	0.8096	0.5212
Filters	34	25.86	32.56	0.8292	1.0888
Poisson	PSNR	MSE	WPSNR	SSIM	TIME
DWT	33.32	30.23	35.03	0.8094	0.5388
Filters	34.05	25.56	32.67	0.8285	1.066

Table 2: Table Showing Different PSNR, MSE, WPSNR, SSIM and Run Time for Image 2

Salt & pepper	PSNR	MSE	WPSNR	SSIM	TIME
DWT	31.83	42.59	31.75	0.6969	1.76
Filters	31.71	43.81	29.96	0.8112	1.304
Bivariate Shrinkage	47.059	1.274	38.12	0.8302	0.2085
Dual Tree with CWT	47.03	1.288	38.16	0.831	0.6632
Gaussian	PSNR	MSE	WPSNR	SSIM	TIME
DWT	28.15	91.43	29.26	0.766	0.5541
Filters	29.81	67.85	28.69	0.8039	1.0996
Bivariate Shrinkage	30.12	63.14	33.29	0.8974	0.2229
Dual Tree with CWT	30.15	59.97	33.56	0.9169	0.67
Speckle	PSNR	MSE	WPSNR	SSIM	TIME
DWT	29.16	78.81	30.15	0.7983	0.9164
Filters	29.42	74.18	28.46	0.8091	1.153
Bivariate Shrinkage	30.12	56.33	33.59	0.9336	0.2878
Dual Tree with CWT	30.7	55.23	33.61	0.9385	5.4801
Poisson	PSNR	MSE	WPSNR	SSIM	TIME
DWT	30.12	63.2	31.6	0.7988	0.5402
Filters	30.81	53.84	29.3	0.8106	1.092
Bivariate Shrinkage	33.85	26.79	37.81	0.9705	0.2231
Dual Tree with CWT	34.17	24.89	38	0.977	0.661

Comparison with existing method

Table 3: Table Showing Different PSNR, MSE, WPSNR, SSIM

Method/parameter	PSNR	MSE	SSIM	ET
HF (using CWM)	25.49234	34.84196	0.98692	2.434407
Proposed method	33.98	25.96	.9979	1.7435

## 5. Conclusion

However selection of the actual denoising procedure plays an important role, it is essential develop to experiment and compare the methods. Finally it is also possible to combine our method with other to get high quality of result. Along with these points we combine various filters namely, average filter, median filter and diffusion filter with DWT. The result of wavelet threshold are fed into the sequence of filter (average, median and diffusion) and the image denoising result are found to be improved on most of the image type. As the preprocessing filter is designed in the wavelet domain, it provides a composite effect on improving the denoising performance of given hybrid method at high frequencies. Experimental results prove that the method not only improves the denoising performance in terms of PSNR, SSIM, and visual presentation, but also it reduces the execution time required for denoising.

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